Calcium-dependent copper redistributions in neuronal cells revealed by a fluorescent copper sensor and X-ray fluorescence microscopy

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Dynamic fluxes of s-block metals like potassium, sodium, and calcium are of broad importance in cell signaling. In contrast, the concept of mobile transition metals triggered by cell activation remains insufficiently explored, in large part because metals like copper and iron are typically studied as static cellular nutrients and there are a lack of direct, selective methods for monitoring their distributions in living cells. To help meet this need, we now report Coppersensor-3 (CS3), a bright small-molecule fluorescent probe that offers the unique capability to image labile copper pools in living cells at endogenous, basal levels. We use this chemical tool in conjunction with synchrotron-based microprobe X-ray fluorescence microscopy (XRFM) to discover that neuronal cells move significant pools of copper from their cell bodies to peripheral processes upon their activation. Moreover, further CS3 and XRFM imaging experiments show that these dynamic copper redistributions are dependent on calcium release, establishing a link between mobile copper and major cell signaling pathways. By providing a small-molecule fluorophore that is selective and sensitive enough to image labile copper pools in living cells under basal conditions, CS3 opens opportunities for discovering and elucidating functions of copper in living systems.

fluorescent sensor | molecular imaging | mobile metals | transition metal signaling

Metals are essential components of all living cells, and in many cases cells trigger and utilize dynamic metal movements for signaling purposes. Such processes are well established for alkali and alkaline earth metals like potassium, sodium, and calcium (1–3) but not for transition metals like copper and iron, which are traditionally studied as their roles as static cofactors in enzymes (4–6). We have initiated a program aimed at exploring the concept of mobile transition metals and their contributions to cell physiology and pathology, and in this context, brain neurons offer an attractive model for this purpose owing to their widespread use of potassium and sodium ion channels and calcium release for signaling events (7), as well as a high requirement for copper and iron to meet their steep oxidative demand (8–12). Indeed, the brain needs much higher levels of copper compared to other parts of the body under normal physiological conditions (9, 12), but at the same time mishandling of neuronal copper stores and subsequent oxidative stress and damage events are connected to a variety of neurodegenerative ailments, including Menkes and Wilson’s diseases (13, 14), Alzheimer’s disease (15–17), familial amyotrophic lateral sclerosis (18, 19), and prion-mediated encephalopathies (20, 21). Previous work hints at the importance of exchangeable copper in neurophysiology, including observations of 64Cu efflux from stimulated neurons (22, 23), export of Cu from isolated synaptosomes (24), and elevated susceptibility of neurons to excitotoxic insult with copper chelation (25), but none of these reports show direct, live-cell monitoring of spatial copper distributions during various stages of neural activity.

Along these lines, molecular imaging with copper-responsive fluorescent sensors offers a potentially powerful methodology for interrogating its cell biology by allowing the specific tracking of copper pools in living cells with spatial and temporal resolution (12, 26–32). In this regard, analogous tools have revolutionized the study of calcium in a variety of biological settings (1) and hold promise for interrogating other cellular metals (26). However, fluorescence-based sensing of Cu2+, the oxidation state stabilized in reducing cytosolic environments, presents several additional challenges that make it more difficult to detect compared to other abundant metal ions in cells (e.g., Na+, K+, Ca2+, Mg2+, Zn2+). The most prominent of these challenges include (i) redox specificity over Cu2+, the other major oxidation state for biological copper, (ii) the propensity for Cu+ in water to disproportionate to Cu2+ and Cu metal, and (iii) the ability of Cu+ to quench fluorescence by electron and/or energy transfer. Indeed, of the growing number of reported strategies for fluorescence copper detection (12, 26), only three synthetic sensors, CTAP-1 (29), CS1 (30, 31), and RCS1 (32), and two protein-based sensors (33, 34) have been validated for live-cell imaging with Cu++. Moreover, the relatively low quantum efficiencies of the first-generation synthetic reagents (Φ ≤ 0.14 in Cu2+-bound forms) have limited their use to date for cellular imaging under conditions of prolonged copper overload or depletion.

Here, we present the synthesis, properties, and applications of Coppersensor-3 (CS3), a bright fluorescent sensor that now offers the unique ability to detect labile copper pools at basal, endogenous levels in living cells. This BODIPY-based probe features high selectivity over competing cellular metal ions, including redox differentiation between Cu+ and Cu2+, visible wavelength excitation and emission profiles, and a 75-fold fluorescence turn-on response with high quantum efficiency (Φ = 0.40) for Cu2+ detection. By using this chemical tool in conjunction with synchrotron-based microprobe X-ray fluorescence microscopy (XRFM) in a combined imaging study, an approach that has been successfully employed for monitoring resting copper distributions in mammalian cells (29), we have discovered that neuronal cells trigger a marked translocation of copper pools from their cell bodies to extended outer processes when activated by depolarization. Moreover, additional CS3 and microprobe XRFM studies show that these dynamic copper movements are dependent on the


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release of calcium, establishing a link between mobile copper and major cell signaling pathways. The combined advances in optical brightness and turn-on response for CS3 afford a host of opportunities for studying the cell biology of copper by providing the ability to visualize labile copper pools in living cells under basal and stimulated conditions.

Results and Discussion
Design, Synthesis, and Spectroscopic Evaluation of Coppersensor-3 (CS3), a Bright Fluorophore for Selective Cu(I) Detection. We previously reported Coppersensor-1 (CS1), a first-generation, selective turn-on fluorescent sensor for aqueous Cu⁺ with visible excitation and emission profiles, and demonstrated its utility for live-cell imaging (30). This reporter shows good selectivity for Cu⁺ over other cellular metal ions at physiologically relevant concentrations, a robust 10-fold fluorescence enhancement upon Cu⁺ complexation, and allows for the visualization of Cu⁺ in live mammalian cells under conditions of acute copper overload. However, attempts to use CS1 to interrogate the dynamics of endogenous cellular copper pools at basal levels were limited by the relatively low quantum yield of the CS1:Cu⁺ complex (Φ = 0.13). Seeking to maintain high Cu⁺ specificity while improving optical brightness values and turn-on responses, we reasoned that increasing electron density on the fluorophore would favor a greater turn-on enhancement through a chromic shift in emission maximum to 548 nm (Fig. 2). Values represent a significant improvement over the first-generation Coppersensor-1 (CS1), a first-generation, selective Cu⁺-dye complex. Nagano’s laboratory has previously shown that substitution of fluoro substituents with methoxy groups on the boron center of BODIPY fluorophores offers a practical strategy for tuning electronic properties of these fluoroscent dyes (35). Fig. 1 details the synthetic route to Coppersensor-3 (CS3) based on these design considerations.

Spectroscopic analysis of apo CS3 in 20 mM HEPES buffered to pH 7 reveals one major peak in the visible region at 550 nm (ε = 3.1 × 10⁴ M⁻¹ cm⁻¹) with a shoulder at 511 nm. Maximal emission occurs at 560 nm with weak fluorescence (Φ = 0.007). Addition of Cu⁺ leads to a blue shift in the absorption band to 540 nm (ε = 4.6 × 10⁴ M⁻¹ cm⁻¹) and a large 75-fold increase in fluorescence intensity (Φ = 0.40), with a corresponding hypsochromic shift in emission maximum to 548 nm (Fig. 2). These values represent a significant improvement over the first-generation CS1 dye (Cu⁺-bound Φ = 0.13, 10-fold turn-on response) that implies for its practical utility in cell imaging experiments (vide infra). Binding analysis using the method of continuous variations (Job’s plot) indicates that a 1:1 Cu⁺:dye complex is responsible for the turn-on fluorescence response observed for CS3 (SI Text). The apparent dissociation constant for the CS3:Cu⁺ complex is 8.9(3) × 10⁻¹⁴ M in HEPES buffer at pH 7 (SI Text).

CS3 exhibits high selectivity for Cu⁺, even in the presence of physiologically relevant concentrations of competing metal ions (Fig. 2B). The fluorescence response of CS3 to Cu⁺ is not affected by the presence of 2 mM Ca⁺², Mg⁺², and Zn⁺², nor do these metal ions cause increases in the fluorescence signal. Moreover, other biologically abundant transition metal ions (50 μM Co⁺², Fe⁺³, Mn⁺², or Ni⁺²) do not trigger false positives, nor do they interfere with Cu⁺-induced fluorescence enhancements for CS3. More importantly, 50 μM Cu⁺⁻ neither causes a fluorescence increase nor hinders the response of CS3 to Cu⁺⁻, indicating that CS3 maintains oxidation state specificity for Cu⁺ over Cu⁺²⁻. Finally, owing to the thioether groups in the sensor we have included a panel of trace soft heavy metal ions for selectivity studies, including Hg⁺²⁻, Ag⁺, Tl⁺, and Pb⁺²⁻ (6) (SI Text). Of these heavy metal ions, CS3 does show some turn-on response to Ag⁺ at high, nonphysiological levels, but the addition of Cu⁺ reveals that Cu⁺ can displace Ag⁺ from the sensor. The large fluorescent turn-on response of CS3 to Cu⁺, in conjunction with its high selectivity in the presence of interfering ions, suggests that this tool is a promising reagent for imaging basal levels of exchangeable Cu⁺ pools in living cells.

Fig. 1. Synthesis of CS3.
To evaluate the spatial distributions of labile Cu intracellular Cu neuronal cells under basal conditions, we measured the emission metal ions. Bars represent the final integrated fluorescence response (sequent addition of 4 associated cultured neurons stained with 2 homeostasis in brain neurons. To this end, live hippocampal distributions, we then sought to use this chemical tool to probe copper is sensitive enough to visualize labile pools under basal condition.

Source of the Argonne National Laboratory. XRFM affords, without any added reagents, a direct method for measuring total copper and other element distributions by their synchrotron-induced X-ray fluorescence signatures (29, 37–40). In particular, the instrument at the 2-ID-E beamline at the Advanced Photon Source of the Argonne National Laboratory boasts a spatial resolution of 200 nm, which makes it appropriate for examining the subcellular elemental distributions of single cells (41). We emphasize that the XRFM method measures total element content on fixed samples, thus providing a complementary approach to live-cell imaging of labile metal pools using fluorescent sensors. Moreover, the combination of small-molecule fluorescence imaging and XRFM has been exploited previously to provide a coherent picture of copper homeostasis in resting mammalian cells, setting the stage for studies of copper homeostasis in dynamic and stimulated situations in the present study (26, 27).

For the XRFM experiments, we utilized the same types of hippocampal neurons employed for the live-cell CS3 imaging studies but cultured on silicon nitride windows. These neuronal cell cultures were incubated either in buffer for 2 min as a baseline control or in buffer supplemented with 50 mM KCl to trigger their depolarization. The cells were then promptly fixed with paraformaldehyde (PFA) and examined by XRFM (Fig. 4). The elemental maps of total copper, zinc, and phosphorus pools are shown for baseline control neurons treated with buffer prior to fixation (Fig. 4 B–D). Phosphorus and zinc signals are concen-

Fig. 2. Spectroscopic responses and selectivity of CS3. All spectra were acquired in 20 mM HEPES, pH 7, at 25 °C. (A) Fluorescence response of 4 μM CS3 to Cu⁺. Spectra shown are for buffered [Cu⁺] of 0, 0.3, 0.5, 0.8, 1.0, 1.5, 2.0, 2.5, 3.0, 3.5, and 4.0 μM. (B) Fluorescence responses of CS3 to various metal ions. Bars represent the final integrated fluorescence response (FI) over the initial integrated emission (FI). White bars represent the addition of an excess of the appropriate metal ion (2 mM for Ca²⁺, Mg²⁺, and Zn²⁺, 50 μM for all other cations) to a 4 μM solution of CS3. Black bars represent the subsequent addition of 4 μM Cu⁺ to the solution. Excitation was provided at 530 nm, and the collected emission was integrated over 540 to 700 nm.

Discovery of Depolarization-Induced Movements of Copper Pools in Neurons with Live-Cell CS3 Molecular Imaging. With data showing that CS3 is capable of reporting dynamic changes in endogenous intracellular Cu⁺ stores by molecular imaging and that this probe is sensitive enough to visualize labile pools under basal conditions, we then sought to use this chemical tool to probe copper homeostasis in brain neurons. To this end, live hippocampal dissociated cultured neurons stained with 2 μM CS3 show a diffuse fluorescent signal pattern, localized mainly in the soma (Fig. 4A). To evaluate the spatial distributions of labile Cu⁺ pools in these neuronal cells under basal conditions, we measured the emission intensity ratio of dendritic copper to somatic copper regions (DCu⁺∶SCu⁺). Quantification of the dendritic and somatic fluorescence intensity signals provides a DCu⁺∶SCu⁺ ratio signal of 0.24 ± 0.04 in these resting neurons.

We then moved on to characterize the distribution of labile copper pools in activated neuronal cells. Interestingly, we observed that neurons treated with 50 mM KCl for 2 min to induce their depolarization and stained with 2 μM CS3 show a marked redistribution of labile copper pools from their somatic cell bodies to peripheral processes, quantified by a patent increase in DCu⁺∶SCu⁺ ratio to 0.35 ± 0.04 (Fig. 4E). These imaging data, which provide direct evidence that the spatial distributions of copper change upon neuronal activation, suggest that the redistribution of labile copper pools might be a result of a rise in dendritic levels and/or a decrease in somatic levels.

**XRFM Provides an Independent and Complementary Method for Visualizing Mobile Copper Triggered in Depolarized Neuronal Cells.** To study mobile copper in neuronal cells using an independent technique as well as verify our CS3-based molecular imaging results, we performed XRFM experiments at the Advanced Photon Source of the Argonne National Laboratory. XRFM affords, without any added reagents, a direct method for measuring total copper and other element distributions by their synchrotron-induced X-ray fluorescence signatures (29, 37–40). In particular, the instrument at the 2-ID-E beamline at the Advanced Photon Source of the Argonne National Laboratory boasts a spatial resolution of 200 nm, which makes it appropriate for examining the subcellular elemental distributions of single cells (41). We emphasize that the XRFM method measures total element content on fixed samples, thus providing a complementary approach to live-cell imaging of labile metal pools using fluorescent sensors. Moreover, the combination of small-molecule fluorescence imaging and XRFM has been exploited previously to provide a coherent picture of copper homeostasis in resting mammalian cells, setting the stage for studies of copper homeostasis in dynamic and stimulated situations in the present study (26, 27).

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Fig. 3. Molecular imaging of endogenous basal Cu in HEK 293T cells with CS3. (A) Control HEK 293T cells, (B) HEK 293T cells supplemented with 200 μM BCS in the growth medium for 20 h at 37 °C, and (C) HEK 293T cells treated with 100 μM TEMEA for 10 min. A, B, and C were stained with 2 μM CS3, 5 μM Hoechst 33342, and DMSO vehicle for TEMEA for 10 min at 37 °C in DMEM. (D) Graph showing the quantification of mean fluorescence intensity of each condition normalized to the control condition (n = 5 fields of cells per condition). Error bars represent the SEM. Asterisk (*) indicates P < 0.01 compared to control cells.
Brain neurons trigger movements of intracellular copper pools. Also in line with the CS3 imaging data, neurons depolarized with 50 mM KCl show a significant change in cellular copper signal that is more diffuse in the depolarized brain cells compared to resting ones (Fig. 4A–H), with copper pools displaying a marked redistribution from the cell body to peripheral processes. In contrast to the copper channel, similar elemental distributions of phosphorus and zinc are observed in the KCl-depolarized neurons compared to their unstimulated counterparts, revealing the relative mobility of copper pools in this model under these conditions. Quantification of the dendritic:somatic copper ratio from XRFM data collected from multiple Advanced Photon Source beam runs over 4 y shows a statistically significant increase in KCl-stimulated neurons (0.84 ± 0.04) compared to basal, untreated neurons (0.54 ± 0.07) (Fig. 4I). Taken together, the CS3 and XRFM imaging experiments provide two independent methods that have allowed us to discover and establish that brain neurons trigger movements of intracellular copper pools upon their activation, causing a significant redistribution of neuronal copper stores from their somatic cell bodies to peripheral processes.

**CS3 Imaging and XRFM Show that Cellular Copper Movements are Dependent on Calcium Release.**

We next used CS3-based molecular imaging and XRFM to probe the effects of intracellular calcium release, a primary consequence of depolarization-induced neural activity, on the observed cellular copper movements. Multiple and distinct types of treatments to alter calcium release, including direct metal chelation or inhibition of cellular calcium entry channels or intracellular receptors, support a relationship between mobile copper and calcium signaling in this model.

First, intracellular calcium rises in neurons were blocked by treatment with the established intracellular Ca\(^{2+}\) chelator BAPTA, delivered in its membrane-permeable acetoxymethyl form BAPTA-AM; this prochelator undergoes rapid hydrolysis by intracellular esterases to produce BAPTA (42). As shown in Fig. 5, Ca\(^{2+}\) chelation prevents KCl-induced redistribution of neuronal copper pools, as the observed \(D_{\text{Cu:S}}\) ratio in BAPTA-AM–treated hippocampal neurons treated with 50 mM KCl in ECS buffer for 2 min and then stained with 2 \(\mu\)M CS3 for 10 min. (B–D) Rat hippocampal neurons treated with ECS buffer for 2 min, fixed with 4% PFA and imaged by XRFM. Images shown are for (B) Cu, (C) Zn, and (D) P channels. (E) Live primary rat hippocampal neurons treated with 50 mM KCl in ECS buffer for 2 min and then stained with 2 \(\mu\)M CS3 for 10 min. (F–H) Rat hippocampal neurons treated with 50 mM KCl in ECS buffer for 2 min and then fixed with 4% PFA and imaged by XRFM. Images shown are for (F) Cu, (G) Zn, and (H) P channels. (I) Graph showing the blinded quantification of CS3-derived dendrite:soma fluorescence ratios for resting and depolarized neurons (\(n = 18\)). Error bars represent SEM (\(P = 0.09\)). (J) Graph showing the XRF dendrite:soma fluorescence ratios for resting and depolarized neurons. Error bars represent SEM.

**Fig. 4.** Molecular imaging of Cu distributions in resting and depolarized rat hippocampal neurons with CS3 and XRFM. (A) Live primary rat hippocampal neurons treated with extracellular solution (ECS) buffer for 2 min and then stained with 2 \(\mu\)M CS3 for 10 min. (B–D) Rat hippocampal neurons treated with ECS buffer for 2 min, fixed with 4% PFA and imaged by XRFM. Images shown are for (B) Cu, (C) Zn, and (D) P channels. (E) Live primary rat hippocampal neurons treated with 50 mM KCl in ECS buffer for 2 min and then stained with 2 \(\mu\)M CS3 for 10 min. (F–H) Rat hippocampal neurons treated with 50 mM KCl in ECS buffer for 2 min and then fixed with 4% PFA and imaged by XRFM. Images shown are for (F) Cu, (G) Zn, and (H) P channels. (I) Graph showing the blinded quantification of CS3-derived dendrite:soma fluorescence ratios for resting and depolarized neurons (\(n = 18\)). Error bars represent SEM (\(P = 0.09\)). (J) Graph showing the XRF dendrite:soma fluorescence ratios for resting and depolarized neurons. Error bars represent SEM.

**Fig. 5.** (A) Rat hippocampal neurons treated with ECS buffer for 2 min with 10 \(\mu\)M BAPTA-AM and then stained with 2 \(\mu\)M CS3 for 10 min. (B–D) Rat hippocampal neurons treated with ECS buffer with 10 \(\mu\)M BAPTA-AM for 2 min and then fixed with 4% PFA and imaged by XRFM. Images shown are for (B) Cu, (C) Zn, and (D) P channels. (E) Live primary rat hippocampal neurons treated with 50 mM KCl in ECS buffer with 10 \(\mu\)M BAPTA-AM for 2 min and then stained with 2 \(\mu\)M CS3 for 10 min. (F–H) Rat hippocampal neurons treated with 50 mM KCl in ECS buffer with 10 \(\mu\)M BAPTA-AM for 2 min and then fixed with 4% PFA and imaged by XRFM. Images shown are for (F) Cu, (G) Zn and (H) P channels. (I) Graph showing the blinded quantification of CS3-derived dendrite:soma fluorescence ratios for BAPTA-AM–treated (\(n = 22\)) and BAPTA-AM/KCl–treated (\(n = 16\)) neurons. Error bars represent SEM. (J) Graph showing the XRF dendrite:soma fluorescence ratios for resting and depolarized BAPTA-AM–treated neurons. Error bars represent SEM.

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ter, KCl-depolarized neurons is similar to unstimulated samples as measured by CS imaging. The collective data provide evidence that transient elevation of intracellular calcium levels is required upstream of depolarization-induced copper translocation and provide a link between mobile copper and calcium, a major modulator of cell signaling pathways.

We then performed XRFM experiments to independently establish that calcium signaling is required to trigger activity-dependent copper movements in these neuronal cell models. Neurons were pretreated with BAPTA-AM and either mock treated with BAPTA-AM-containing buffer for 2 min or with buffer containing 50 mM KCl and 10 μM BAPTA-AM. Notably, the XRFM images directly show that the levels and distributions of cellular copper are not perturbed by BAPTA treatment. Moreover, XRFM analysis of these cells indicated no significant differences in copper distributions between cells that had been treated with only buffer (Fig. 5 B–D) or cells that had been depolarized (Fig. 5 F–H). These results, in conjunction with the CS3 imaging of live neurons, reinforce the link between calcium signaling and mobile copper pools in brain cell systems.

In further support of the aforementioned experiments, we then proceeded to alter calcium signaling pathways using reagents that are not metal chelators. First, we added dantrolene, a well-established drug that decreases intracellular calcium levels by binding to the ryanodine receptor (43, 44). As shown in Fig. 6, dantrolene also blocks KCl-induced redistribution of neuronal copper pools, as the observed $D_{C_u}/S_{C_u}$ ratio in dantrolene-treated, KCl-depolarized neurons is similar to unstimulated samples as monitored by CS imaging. Next, we added nifedipine, a classic dihydropyridine calcium channel blocker that inhibits transmembrane flux of extracellular calcium ions (44). Unlike the dantrolene and BAPTA treatments, nifedipine at this dose does not diminish the KCl-induced mobilization of labile copper pools to the same extent. Finally, the combined application of both dantrolene and nifedipine also abolishes the depolarization-triggered soma-to-dendrite movements of neuronal copper. By showing that interfering with calcium entry or intracellular receptor pathways can also block depolarization-induced movements of neuronal copper, these additional lines of evidence provide further support for a link between mobile copper and calcium signaling.

Concluding Remarks

Dynamic metal fluxes triggered by physiological stimulation are well established for alkali and alkaline earth metals like potassium, sodium, and calcium in a wide range of cell types but are insufficiently explored for transition metals. In this work, we utilize a fluorescent sensor and XRFM imaging to directly show that movements of copper pools are triggered by cell activation in a neuronal model, suggesting that this transition metal nutrient can also participate as a dynamic component for essential physiological functions. Indeed, cellular copper uptake and release is kinetically rapid (45), and growing evidence highlights the importance of orchestrating transient copper accumulation, compartmentalization, and efflux events within subcellular compartments at a molecular level (13, 28, 46–51). The brain’s high copper demand, along with growing connections between copper misregulation and neurodegenerative diseases, point to the particular importance of understanding copper homeostasis in this unique biological system.

In this report, we have presented CS3, a fluorescent sensor where improvements in turn-on response and quantum efficiency give this probe a unique ability to monitor labile copper pools in living cells at basal and copper-depleted conditions. We have used this chemical probe in conjunction with XRFM in a combined imaging study to discover that neuronal cells move significant pools of copper from their somatic cell bodies to extended outer processes when activated by depolarization. Moreover, additional CS3 and XRFM imaging experiments establish that the observed copper redistributions are dependent on calcium release, showing that mobile copper is linked to a major hub of cell signaling pathways and presages a wide range of possibilities for exploring copper and calcium crosstalk.

The ability to directly monitor mobile pools of copper during different stages of neuronal cell activity highlights the combined use of live-cell molecular imaging for visualizing exchangeable copper pools along with XRFM to characterize total copper content as a synergistic approach to study metal homeostasis.

![Graph showing the blinded quantification of CS3-derived dendrites:soma fluorescence ratios for resting, depopolarized, and inhibitor-treated neurons.](image)

**Fig. 6.** Molecular imaging of Cu distributions in resting, depolarized, and inhibitor-treated rat hippocampal neurons with CS3. (A) Live primary rat hippocampal neurons treated with ECS buffer for 10 min, (B) treated with ECS buffer with 30 μM dantrolene for 10 min, (C) treated with ECS buffer with 100 μM nifedipine for 10 min, (D) treated with ECS buffer with 30 μM dantrolene and 100 μM nifedipine for 10 min, (E) treated with 90 mM KCl in ECS buffer for 2 min, (F) treated with 30 μM dantrolene in ECS buffer for 10 min and then 90 mM KCl in ECS buffer for 2 min, (G) treated with 100 μM nifedipine in ECS buffer for 10 min and then 90 mM KCl in ECS buffer for 2 min, and (H) treated with 30 μM nifedipine and 100 μM dantrolene in ECS buffer for 10 min and then 90 mM KCl in ECS buffer for 2 min. (G) Graph showing the blinded quantification of CS3-derived dendrites:soma fluorescence ratios for resting, depopolarized, and inhibitor-treated neurons ($n \geq 11$). Error bars represent the SEM. Asterisk (*) indicates $P < 0.05$. 

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in a native cellular context. Our findings, taken together with previous reports showing accumulation of mitochondria to neuronal filopodia and dendritic spines upon repeated depolarization (52), reversible trafficking of the P-type ATPase ATP7A from the perinuclear trans-Golgi to neuronal processes by NMDA receptor activation (23), and axonal localization of ATP7A potentially involved in process guidance (53, 54), point to the intriguing possibility that subcellular compartmentalization and transient reorganization of copper stores is essential to tuning dynamic neuronal activity. Furthermore, the requirement for calcium release to trigger copper movements provides an entry for connecting copper to canonical signal transduction pathways. We are actively pursuing an understanding of mobile copper as a potential new metal signal in the context of neuronal activity and other fundamental physiological processes.

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